### Journal Pre-proof

Identifying consistent biomechanical parameters across rising-to-walk subtasks to inform rehabilitation in practice: A systematic literature review

Gareth D Jones (Conceptualization) (Methodology) (Software)<ce:contributor-role>Formal Analysis) (Investigation)<ce:contributor-role>Data Curation)<ce:contributor-role>Writing – Original Draft)<ce:contributor-role>Writing – Review and Editing) (Visualization)<ce:contributor-role>Project Administration), Gareth L Jones<ce:contributor-role>Formal Analysis) (Investigation)<ce:contributor-role>Writing – Review and Editing), Darren C James (Conceptualization) (Methodology)<ce:contributor-role>Writing – Review and Editing) (Visualization) (Supervision), Michael Thacker (Conceptualization) (Methodology)<ce:contributor-role>Writing – Review and Editing) (Supervision), David A Green (Conceptualization) (Methodology) (Validation) (Resources)<ce:contributor-role>Writing – Review and Editing)<ce:contributor-role>Project Administration) (Supervision)

GAIT POSTURE

PII:	S0966-6362(20)30578-6
DOI:	https://doi.org/10.1016/j.gaitpost.2020.10.001
Reference:	GAIPOS 7921
To appear in:	Gait & Posture
Received Date:	20 May 2020
Revised Date:	7 August 2020
Accepted Date:	2 October 2020

Please cite this article as: D Jones G, L Jones G, James DC, Thacker M, A Green D, Identifying consistent biomechanical parameters across rising-to-walk subtasks to inform rehabilitation in practice: A systematic literature review, *Gait and amp; Posture* (2020),

### doi: https://doi.org/10.1016/j.gaitpost.2020.10.001

This is a PDF file of an article that has undergone enhancements after acceptance, such as the addition of a cover page and metadata, and formatting for readability, but it is not yet the definitive version of record. This version will undergo additional copyediting, typesetting and review before it is published in its final form, but we are providing this version to give early visibility of the article. Please note that, during the production process, errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

© 2020 Published by Elsevier.

Identifying consistent biomechanical parameters across rising-to-walk subtasks to inform rehabilitation in practice: A systematic literature review

### **Author Names:**

### Gareth D Jones<sup>1,2</sup>

<sup>1</sup>Centre for Human and Applied Physiological Sciences (CHAPS), Shepherd's House, Guy's Campus, King's College London, London SE1 1UL, UK. <sup>2</sup>Physiotherapy Department, 3rd Floor Lambeth Wing, St Thomas' Hospital, Westminster Bridge Road, Guy's & St Thomas' NHS Foundation Trust, London, SE1 7EH, UK. gareth.jones@gstt.nhs.uk

### Gareth L Jones<sup>2</sup>

<sup>2</sup>Physiotherapy Department, 3rd Floor Lambeth Wing, St Thomas' Hospital, Westminster Bridge Road, Guy's & St Thomas' NHS Foundation Trust, London, SE1 7EH, UK. gareth.jones2@gstt.nhs.uk

### Darren C James3

<sup>3</sup>Sport and Exercise Science Research Centre, London South Bank University, 103 Borough Road, London, SE1 0AA, UK. jamesd6@lsbu.ac.uk

### Michael Thacker<sup>i1,2</sup>

<sup>1</sup>Centre for Human and Applied Physiological Sciences (CHAPS), Shepherd's House, Guy's Campus, King's College London, London SE1 1UL, UK

<sup>2</sup>Physiotherapy Department, 3rd Floor Lambeth Wing, St Thomas' Hospital, Westminster Bridge Road, Guy's & St Thomas' NHS Foundation Trust, London, SE1 7EH, UK. michael.thacker@lsbu.ac.uk

### David A Green<sup>ii1</sup>

<sup>1</sup>Centre for Human and Applied Physiological Sciences (CHAPS), Shepherd's House, Guy's Campus, King's College London, London SE1 1UL, UK david.green@esa.int

<sup>i</sup>Present Address: School for Health and Social Care, London South Bank University, London, United Kingdom

<sup>ii</sup>Present Address1: European Astronaut Centre, Directorate of Human Spaceflight and Robotic Exploration Programmes (D/HRE), European Space Agency, Cologne, Germany

Present Address 2: KBRwyle GmbH, Albin Köbis Straße 4, Cologne, 51147, Germany

### **Corresponding Author:**

Gareth D Jones Clinical Lead Physiotherapist - Rehabilitation Physiotherapy Department, 3rd Floor Lambeth Wing, St Thomas' Hospital, Westminster Bridge Road, Guy's & St Thomas' NHS Foundation Trust, London, SE1 7EH, UK. Tel: +44 (0) 2071885082 ORCID: 0000-0001-5516-9418 gareth.jones@gstt.nhs.uk

### Highlights

- Normal rising-to-walk (RTW) performance is fluid, but is non-fluid with pathology
- Rehabilitation could be tested if RTW controlled performance variables were known
- Consistent variables regardless of healthy RTW performance represent candidates
- In this review of 9 studies, no compelling evidence of consistency was found
- Studies designed to confirm consistent biomechanical variables are needed

### 1 Abstract

**Background**: The best approach to rehabilitate the control of everyday whole-body movement (e.g. rise-to-walk) after pathology remains unclear in part because the associated controlled performance variables are not known. Rise-to-walk can be performed fluidly (sit-to-walk) or non-fluidly (sit-to-stand, proceeded by gait-initiation). Biomechanical variables that remain consistent in health regardless of how rise-to walk is performed represent controlled performance variable candidates which could monitor rehabilitative change.

**Research Question:** To determine if any biomechanical parameters remain consistent across rising-to-walk (RTW) subtasks (sit-to-stand, gait-initiation, and sit-to-walk) in healthy adults for purposes of movement control assessment in clinical practice.

**Methods**: Data sources included Medline, Cinahl, and Scopus databases, and the grey literature. Study Selection was based on eligibility criteria and must have reported spatiotemporal, kinematic and/or kinetic biomechanical parameters featuring >1 RTW subtask. Data Extraction and Synthesis; standardised-mean-differences (SMDs) were calculated (pooled if replicated in >1 study) for each parameter. Consistency was determined if SMD95%CIs included the zero-effect line.

**Results:** Nine studies (n=99) were included ( $40\pm7.5$ yrs). Seven parameters were replicated in >1 study and subjected to meta-analysis (fixed-effect model). Two were consistent between sit-to-stand and sit-to-walk: flexion-momentum time (M(95%CI)= 0.055(-0.423 to 0.533); p=0.823) and peak whole-body-centre-of-mass vertical velocity (M(95%CI)= -0.415(-0.898 to 0.069); p= 0.093); and centre-of-pressure to whole-body-centre-of-mass distance at toe-off (M(95%CI)= -0.137(-0.712 to 0.439); p= 0.642) between gait-initiation and sit-to-walk. Another 20 parameters were consistent based on single-study SMDs.

**Significance**: Consistent parameters might exist across RTW subtasks. However, the evidence is based on few studies with small samples and variable RTW protocols. Future studies designed to confirm consistency using a standardised RTW protocol are needed.

**Keywords:** early ambulation; gait-initiation; rehabilitation research; systematic review; sit-to-stand; sit-to-walk

### **2** Introduction

Transitional movements are considered to occur whenever rhythmic (e.g. walking or running) or sedentary movements (e.g. lying, sitting, or standing) are combined [1], although there is no consensus upon a standard definition. They are complex because an individual is not only required to control the propulsive forces that move their body segments but must simultaneously maintain their balance during the transition too. Transitional movements are therefore challenging and potentially destabilising movement tasks, for which an individual's sensorimotor system requires sufficient resources in order to control [2].

Rising-to-walking (RTW) is an everyday transitional movement executed daily on average 49 times in healthy people [3] and incorporates two cardinal subtasks; firstly sit-to-stand (STS), and secondly the initiation of walking from standing (gait initiation; GI). A healthy person can execute a continuous version of RTW where the transition of rising (STS), through GI, and into walking forward occurs fluidly and is known as sit-to-walk (STW). Healthy people can also execute another version where the subtasks are performed consecutively but independently and may be partially (hesitant-STW) or entirely separated (separated-STW) as part of a normal dual or combination task [3]. These are collectively known as sit-to-stand-and-walk (STSW) [4], where a pause separates STS from GI. STW and STSW therefore represent the extremes of RTW behaviour.

The assessment of sensorimotor control parameters in ambulatory transitional tasks like RTW can be dichotomised into either the observation of activity with a standardised rating of performance, or the biomechanical measurement of the performance [5]. While performance ratings are ubiquitous in clinical environments due to their time and resource practicalities (e.g. the Berg Balance Scale [6]), biomechanical assessments (e.g. mean anteroposterior centre-of-pressure (COP) displacement velocity [7]) offer less subjectivity despite the disadvantage of often being dependent on lab-based equipment [5].

Rising from sitting commences with movement-onset. The initial priority is to generate anterior whole-body-centre-of-mass (BCOM) momentum which transitions to vertical momentum around the event of seat-off. The phase between movement-onset to seat-off, termed flexion-momentum [8] represents the transition from a dynamically stable three-point, to a two-point base-of-support [9]. Once upright is achieved in STS, forward propulsion is arrested, requiring generation of a substantial (compared to STW) BCOM braking force, manifest as greater peak posterior ground reaction forces (GRFs) [10, 11]. GI, when executed from standing, is characterised by an anticipation phase where the COP is translated posterolaterally towards the swing limb creating a moment arm to propel the BCOM forward [12]. Then, a dynamic execution phase of GI starts at heel-off (HO1) [13]. The first walking step delineated between toe-off (TO1) and initial contact (IC1) [14] with steady-state walking typically established by the end of the second step in healthy individuals, if the transition to walking is continued in a forward direction [15].

A similar COP momentum arm also exists during the anticipation phase of GI in STW, albeit of a lower magnitude due to the BCOM's latent forward momentum generated during initial rising [11, 16]. The challenge in STW is to continue to control rising, despite

GI having already started (GI-onset) before upright is reached [16, 17]. This phase shift is indicative of the rapid and fluid merging of rising and GI around seat-off in STW, and presents a significant motor control challenge [18-20].

Healthy individuals can choose depending on context, attention, purpose or freewill to execute RTW within the range of permutations represented by STS, GI, STW and STSW. This is because healthy people have abundant sensorimotor resources available to them [21]. Put another way, this abundance means that task-specific performance variables can be stabilised by sets of elemental variables that are organised by the central nervous system [22]. For example, leg joint angles (elemental variables) can be organised to stabilise, and therefore control, the BCOM during the stance phase of gait (performance variable) [23]. A biomechanical parameter that remains *consistent* independent of how a complex transitional task like RTW is executed in healthy individuals might therefore represent a controlled performance variable and thus be a candidate proxy for in-tact sensorimotor-system control. This in turn means that discrimination between healthy and pathological sensorimotor-system control is possible by assessment of the consistent parameters(s) during RTW performance.

Consistency in this context is defined as a biomechanical parameter that does not vary (significantly) across RTW performance. Thus, parameters are considered to demonstrate absolute consistency across RTW tasks if the posed null hypothesis (no difference in biomechanical parameter between RTW tasks) is retained following appropriate statistical significance testing. Accordingly, consistent parameters may be used to monitor change in dysfunctional RTW performance, which can enable the development of alternative rehabilitation techniques designed to improve movement control to be tested in clinical practice.

Transitional sensorimotor control is often impaired in older or pathological populations in RTW and its subtasks leading to slower temporal durations of movement phases. For example, lower limb muscular weakness has been shown to prolong STS movement duration in normal aging [24], and stroke impairments have been observed to prolong the relative duration of the transition-phase (seat-off to GI-onset) and overall movement-time in STW [19, 25]. Thus, individuals with pathology execute RTW within a more limited set of permutations more biased towards STSW compared to healthy individuals.

Observations of other *differences* in temporo-spatial, kinematic, or kinetic biomechanical parameters are therefore unsurprising within RTW subtasks (i.e. STS, GI from quietstanding, or STW) between health and pathology. For instance, longer phase durations have been observed during STW in stroke [19], and during GI in Parkinson's disease (PD) [26] compared to healthy individuals. Furthermore, smaller separation distances between the BCOM and the COP have been observed at movement events during STW in healthy older, compared to healthy younger adults [16] during STW in adults with PD compared to healthy older adults [27], and during GI in adults with PD compared to older or younger healthy individuals [28]. In addition, greater momentum and peak mediolateral ground-reaction-forces (GRFs) during STW compared to STS, are examples of differences between RTW subtasks in healthy adults [11, 18]. However, whether any biomechanical parameters exhibit *consistency* throughout the RTW continuum in healthy adults is unclear. This is because explicit evaluations are not-commonly referred to in the literature which means consistency is either not reported at all, or is only implicitly reported in the literature and does not therefore frequently feature in studies' titles, abstracts and discussions.

### Aims

The aim of this systematic review is to determine if any reported spatiotemporal, kinematic and/or kinetic biomechanical parameters remain consistent across rising-to-walk (RTW) subtasks in healthy adults and thereby act as candidate markers to discriminate pathology and evaluate recovery in the rehabilitation of transitions to walking. The objectives are to:

- 1. Systematically identify biomechanical parameters within individual RTW studies that were assessed in at least two RTW subtasks within healthy participants;
- 2. For each biomechanical parameter identified, determine whether any have been reported by more than one study;
- 3. Determine if the biomechanical parameters are consistent between RTW subtasks within or across studies using meta-analysis.

### **3** Methods

A systematic review was performed and its findings are reported in accordance with the Preferred Reporting Items for Systematic Reviews and meta-analyses (PRISMA) statement guidelines [29] (see Supplementary Table 1: PRISMA Checklist).

### Protocol Registration

The protocol for the systematic review was registered with the International Prospective register for Systematic Reviews (PROSPERO; registration no CRD 42019124750).

### Search strategy

The Population/Participants, Intervention, Comparison, and Outcome (PICO) framework was used to define the search strategy concepts [30-32]. Participants must have been healthy human volunteers. Interventions were defined as any instruction to execute any of the following conventional RTW subtasks: sit-to-stand (STS), gait-initiation (GI) and/or sit-to-walk (STW), or other accepted movement instructions (timed-up-and-go test (TUAG) [33], or STSW). The comparison in this case was consistency (as defined) between another RTW sub-task. Studies were included whether healthy participants executing RTW subtasks were part of a control group or not. Single case studies, study protocols, and systematic or narrative reviews were excluded. There was no other restriction on study designs. The outcomes were any spatiotemporal, kinematic and/or kinetic parameter measured in at least 2 RTW subtasks to facilitate determination of consistency.

Electronic databases were searched from database inception to the 15<sup>th</sup> October 2018. Studies were identified by searching electronic databases; MEDLINE (OVID), SCOPUS and CINAHL. Keywords related to the key concepts (healthy adults, RTW subtasks, and kinematic or kinetic biomechanical parameters) were matched to a controlled vocabulary (exploded MeSH terms or subject headings) which was combined with free text terms (see Supplementary Table 2: Example Search Strategy). In addition, grey literature was assessed including postgraduate theses (masters or doctoral using EthOS and WorlCat Dissertation and Thesis (OCLC) databases) in addition to conference abstracts and proceedings [34]. A secondary search, or pearling, of bibliography lists was manually undertaken in publications that fulfilled eligibility criteria.

Two reviewers (GDJ, GLJ) independently performed the electronic database search, subsequent screening, quality assessment, and data extraction. Candidate citations were transferred to a proprietary systematic review platform (Covidence Systematic Review Software. Veritas Health Innovation Ltd. Melbourne, Australia) along with the full text.

### Eligibility criteria

Reviewers screened titles and abstracts using customised criteria including keyword searching in Covidence (see Supplementary Table 3: Title and abstract screening tool). In cases where eligibility was inconclusive, the full text was independently screened.

Disagreements were resolved by discussion, or if consensus not reached by a third experienced reviewer (MT) independently assessing.

### Type of studies

Only studies published in English were included. Single case studies, study protocols, and other systematic or narrative reviews were excluded. There was no other restriction on study design. The search therefore included cross-sectional, cohort studies, prospective cohort or any other experimental study types.

### Type of participants

Human healthy adults aged  $\geq 18$  years were included. No upper age limit was applied to avoid exclusion of patients based on an arbitrary age limit [35], and because consistent biomechanical data *between* RTW tasks *within* healthy participants was the focus of the review.

### Type of biomechanical parameters

Studies that included spatiotemporal, kinematic and/or kinetic parameters measured between reported movement events during any two RTW subtasks were eligible. The parameters encompassed time and spatial measures of the whole-body centre-of-mass (BCOM), centre-of-pressure (COP) or other individual or combined (e.g. head-arm-trunk (HAT)) specific body segments; velocities or momenta, directional components of the ground-reaction-force (GRF), or measures of fluency for example hesitation, coordination, or smoothness [20].

### Study exclusion

Studies investigating participants with reported pathologies affecting normal walking function were excluded unless the study included analysis and separate reporting of a healthy control group. Studies were excluded if only one RTW task was analysed (e.g. STW only [25]) or if a RTW subtask included initial positions other than sitting or standing (e.g. lying-to-walk [3]). If studies assessed walking directions that deviated from forward (e.g. backwards walking [36]) or if studies included walking that included transitions from one surface to another (e.g. stepping up onto a 16cm high box [37]), then they were also excluded.

Studies were also excluded if the main focus was the impact on either a medical, surgical or public health concern using RTW tasks as an assessment (e.g. using timed-STS to assess vitamin D deficiency interventions [38]); or ambulation function using physical performance tests but with no RTW task as a comparison (e.g. using TUAG to assess high-intensity-training effect [39]). Lastly, studies were excluded if reported parameters were dependent on EMG, sensors, or assistive device technology [40].

Risk of bias within individual studies

It was predicted that most literature found in this review would be cross-sectional. Consequently, standardised experimental-design specific quality assessment tools such as PEDro [41, 42] were inappropriate. As a result, study quality was assessed using the Joanna Briggs Institute (JBI) Checklist for Analytical Cross Sectional Studies [43], which is an accepted and valid approach for reporting observational study designs [44, 45]. It uses a 3-point nominal rating system of bias where a score of 0 (zero) is assigned for *low*, 1 for *unclear*, and 2 for a *high risk of bias* for each of the eight quality criteria leading to a total score between zero and 16 (see Supplementary Table 4: Methodological quality assessment tool). To comply with each critical appraisal criterion and be rated low-risk, the study had to meet elements detailed in the criterion description. To be rated a high-risk, the study had to explicitly detail some, but not all, of the criterion description or provide no information. To be rated unclear-risk, the study had to provide some information but without complete clarity as per the criterion description. Cohen's kappa ( $\kappa$ ) [46] was used to determine inter-rater agreement of study quality between the two

reviewers according to accepted rating criteria [47] in each of the 8 quality domains and between the reviewer's total risk of bias score. Disagreements were resolved by discussion, or if consensus not reached via assessment by a third experienced reviewer (MT) independently, yielding final total rating scores. A high risk of bias was concluded if a study returned a final rating of >50% of the total possible score (i.e. >8) [48] and was subsequently excluded from further analysis [43].

### Data extraction

Mean ( $\pm$ SD) study characteristics and biomechanical parameters (see below) were extracted and populated in Covidence by the reviewers independently using customised tables. Disagreements between reviewers were resolved by discussion, or if consensus not reached by assessment by a third experienced reviewer (MT) independently. In cases where the standard error of the mean (SE) but not SD was reported, the SD was calculated as the product of the square-root of the sample size and the SE. If no variance statistic was provided, the range was extracted.

### Study characteristics

Characteristics were collected in order to describe studies' participants and protocols. They comprised: year of publication, aims, number of healthy participants, their gender and handedness, participant height (m), body-mass (kg) or body-mass-index (BMI) and seat height from which participants rose (expressed as either the proportion of knee height (%KH), as an absolute height (m) or as a pre-determined sitting knee angle (°)).

In addition, protocol descriptors were extracted to characterise and compare starting position, task execution and contexts. Pre-determined nominal classifications were used: feet position (standardised/self-selected), arm use (constrained/semi-constrained/self-selected), tempo (controlled/self-selected) and ecological task purpose (upper limb task/walk to target). Other protocol task characteristics extracted were limb-lead, walk distance (m) or alternatively the number of prescribed steps, what RTW subtasks were included and the number of trials undertaken.

### Biomechanical parameters

The number of different biomechanical parameters reported in eligible studies was expected to be high. All parameters measured were initially recorded using the terminology used in the original study. Then, parameters where labelled and classified using a consistent terminology agreed by the reviewers to enable pooled results to be generated across studies.

### Method of analysis

For each extracted biomechanical parameter, the main outcome of interest was the effect size (ES) calculated between two RTW subtasks. The ES was expressed as the standardised mean difference (SMD) and associated 95% confidence intervals (CI).

SMDs were calculated either from data extracted within a single-study if the parameter was only present in one study, or combined across studies if data were extracted in more than one study. SMDs were calculated based on the effect-size (Cohen's *d*) [49]; the proportion of the difference between the mean values and the pooled SD [50]. A minor bias exists in *d* where it tends to overestimate the absolute value of the SMD particularly when sample sizes are small ( $n \le 10$  in each group) [51] which was anticipated. An approximated correction factor (*J*) was therefore calculated [52] and when combined as a product of *d* yielded a corrected SMD ES (Hedge's *g*)[53]. Parameters were considered consistent as defined if the SMD 95% CI included the null value (the line of zero-effect) [52].

Where parameters were shared in 2 or more studies, combined mean effects were calculated to meta-analyse between-task consistency. Fixed-effect analyses were performed because sample sizes and numbers of studies were small. Descriptive analyses of included studies representing the healthy adult population were therefore reported, despite the fact that the studies were likely to have been drawn from researchers working independently where random-effect analyses would be more appropriate [52]. First, the weighted effect size (W) for each study's g was calculated as the reciprocal of  $g^2$ , then the weighted mean effect size (M) was calculated as the sum of the product of g and W divided by the sum of W [52]. If combined effect size 95% CIs included the null value (line of zero-effect), then the null hypothesis was not rejected, and the parameter was considered consistent as defined.

### 4 Results

### Study Selection

A total of 2862 studies were identified through the defined strategies (Figure 1). After 963 duplicates were removed, 1899 titles and then abstracts were screened with 43 studies selected based on eligibility criteria for full-text screening. Thirty studies included upon inspection only one RTW subtask, or steady-state gait or TUAG as the task of interest, and thus were excluded. Two other studies were excluded because they proved unobtainable in full-text despite numerous inter-library requests (2 PhD theses). Two other duplicates were removed. Thus, nine studies were selected for inclusion in the final review.

[Figure 1 here]

### Included study characteristics Design and Participants

All nine included studies employed a cross-sectional cohort design of which one was a short communication paper [54] and two were published abstracts with data not wholly published subsequently in full text papers [55, 56]. A modest number of participants were tested in each study: mean (range) 10.8 (8-13) yielding a total of 99 participants. Two studies failed to report participants' height or mass [55, 57]. Four studies did not report gender distribution [18, 27, 55, 56], whereas in the remainder only 21% were female. In general, studies adopted 5 repeated RTW trials with at least 3m walk distances (Table 1). [Table 1 here]

### Starting position

One study specified a definitive seat height in its experimental protocol [55] while all others standardised it to knee-height, leg-length, or knee-joint angle. Feet positioning was standardised across studies by fixed orientation or positioning and maintained through trials, but two studies allowed a self-selected start position [11, 58]. In five studies, upper limbs were constrained across the trunk or on the waist [11, 18, 27, 56, 57], and the remainder did not include any detail (Table 2).

[Table 2 here]

### Walking and RTW subtasks

Tempo was self-selected throughout, whereas lead-limb was controlled in some studies. Participants self-selected their preferred lead-limb and then maintained it in four studies [11, 18, 27, 55], one specified the left lead-limb [57], one specified both the dominant and non-dominant limb [54], and the remainder provided no details. Only two studies provided any detail of the walking task including an ecologically valid purpose, for example: walking to a target [27] or an upper limb task (switching off a light [54]). All studies included STW as one RTW subtask, five compared it with STS [11, 18, 55, 56, 58], one with GI [57], one with STSW [54], and two compared STW with both STS and GI [10, 27] (Table 2).

### Risk of Bias Within Studies

Across the 9 included studies, the assessors agreed on 45 instances of low bias, 12 unclear, and 7 high bias. However, there were 8 instances where the assessors disagreed on quality. The inter-rater agreement for risk of bias scoring was high,  $\kappa = 0.772$  (95% CI 0.623 to 0.921) (Table 3).

Once the disagreements were resolved (Table 3), the mean ( $\pm$ SD) risk of bias score (from a maximum of 16) was low per study but variable (3.33  $\pm$ 3.81 (range 0-12)). One study was rated with unacceptable bias (risk of bias score 12) and was not included in analyses [56]. Inadequate reporting of healthy group inclusion criteria (criterion 1), participant characteristics (criterion 2) and the omission of confounding variable management (criterion 5) were the most common domains where bias was found across studies. [Table 3 here]

Final biomechanical parameters used for analysis In total, there were 104 biomechanical parameters reported across all studies. However, 52 parameters were either not compared between RTW tasks in healthy participants or data were not possible to extract. For instance, variance statistics were not reported in two studies [57, 58], only partially reported in two others [10, 11] and some parameters were not analysed between-tasks [27, 54, 56]. Thus, 52 biomechanical parameters with between-RTW task data were available for analysis across individual studies (Figure 2).

When the 52 parameters were considered across-studies for replication, three studies (total participants: n=31) analysed flexion-momentum time [11, 27, 54]; three studies (n=27) analysed rise time [11, 54, 55]; three studies analysed peak BCOM vertical velocity (n=31) [10, 27, 54]; two studies (n=22) analysed peak BCOM horizontal velocity and COP-BCOM distance at seat-off and toe-off [27, 54]; and two studies (n=19) analysed swing-limb peak GRF [11, 54]. One biomechanical parameter (flexion-momentum phase duration), unique to the study with high risk of bias [56], was excluded. Thus, it was possible to extract effect-size data for 44 independent biomechanical parameters; 37 unique to individual studies, four replicated across 2 studies, and three parameters replicated across 3 studies (Figure 2). [Figure 2 here]

### Results of Individual Studies

Of the 37 parameters unique to only one RTW comparison study, 20 were consistent (Table 4). These were: 1<sup>st</sup> step width and velocity in GI compared to STW [27]; peak vertical GRF during rising, peak positional stability during steps 1, 2, and 3, and the duration of steps 1, 2, and 3 in STSW compared to STW [54]; peak posterior (braking) GRF and the time from movement-onset to both peak anterior and posterior GRFs in STS compared to STW [55]; time between movement-onset to peak BCOM vertical velocity and the total vertical BCOM displacement in STS compared to STW [10]; and finally, the time between movement-onset and both peak BCOM horizontal and vertical momentum, anteroposterior BCOM and COP position at seat-off, peak BCOM vertical momentum during rising and the peak stance limb vertical GRF during rising in STS compared to STW [11]. Kerr and colleagues [18] reported no consistent parameters between STS and STW.

[Table 4 here]

### Synthesis of Combined Studies

Of the seven biomechanical parameters replicated in more than one study three were common to three studies and four were common to two studies. Of those common to three studies, combined results showed consistency (combined ES 95% CIs included the line of zero effect) between STS and STW in flexion-momentum time (M (95% CI) = 0.053 (-0.423 to 0.533); p=0.823) and in peak BCOM vertical velocity during rising (M (95%

CI) = -0.415 (-0.898 to 0.069); p = 0.093). In contrast, a longer rise-time was found during STS compared to STW((M (95% CI) = 0.950 (0.410 to 1.490); p<0.001) (Figure 3). [Figure 3 here]

In biomechanical parameters common to two studies, the COP-BCOM horizontal distance was consistent between STW and GI at initial toe-off (M (95% CI) = -0.137 (-0.712 to 0.439); p = 0.642) whereas at seat-off it was greater during STS compared to STW (M (95% CI) = 0.610 (0.028 to 1.193); p = 0.040), (Figure 4). [Figure 4 here]

There was no consistency between STS and STW in peak BCOM horizontal velocity during rising where it was faster during STW (M (95% CI) = -1.707 (-2.452 to -0.963); p<0.001) nor in peak swing-limb ground reaction force before the first toe-off event where it was greater during STW (M (95% CI) = -1.350 (-2.033 to -0.667); p<0.001) (Figure 5).

[Figure 5 here]

### Summary of consistent parameters

37 parameters were unique to individual studies and not replicated elsewhere, twenty of which (54%) can be considered consistent by virtue of their 95% CI effect size crossing the line of no effect (zero) (see Table 4 above). Combined with the 3 consistent parameters common to more than one study (see Figure 3 and Figure 4 above), the overall review yielded 23 parameters that were consistent as defined (Table 5). Twenty of the 23 (87%) were consistent between STW and STS (or STSW in one study [54]), with the remaining three parameters (13%) consistent between STW and GI. [Table 5 here]

### **Risk of Publication Bias Across Studies**

A risk of publication bias assessment was planned *a priori* using a funnel plot approach where the relationship between study-size and effect-size is plotted and bias then interpreted by visualisation of any asymmetry in the plot [59]. But, in parameters sharing extracted data, the maximum number of synthesised studies was three. Thus, there was not enough data to undertake an assessment of publication bias in this review.

### **5** Discussion

### Summary of Evidence

The aim of this systematic review was to identify whether any spatiotemporal, kinematic and/or kinetic biomechanical parameters remain consistent independent of how RTW is executed in healthy individuals. If any consistent parameters were identified, they would thereby represent candidate proxies for intact sensorimotor-system control and could potentially discriminate between healthy and pathological sensorimotor-system control and be used to monitor change in dysfunctional RTW performance. This in turn could enable the development of alternative rehabilitation techniques designed to improve impaired movement control to be tested in clinical practice

Consistency was assumed if the 95% confidence intervals around the effect size (MSD from single or combined studies) included the null value (line of zero-effect). Studies analysing only one RTW task, or those only reporting parameters dependent on EMG, sensors, or assistive device technology were excluded.

Abstracts and titles from 43 out of 1899 were full-text screened. Of these, nine studies were found to be eligible and included in the final review. None of the studies stated an aim to assess biomechanical parameter consistency between RTW subtasks in healthy participants. Consequently, spatiotemporal, kinematic and/or kinetic biomechanical parameter data between RTW tasks were extracted to assess for consistency within

### Journal Pre-proof

reviewed studies. One-hundred and four candidate biomechanical parameters were identified between-RTW subtasks. Once parameters with a high risk of bias were removed and replication ensured, the final analysis consisted of 44 parameters: 37 unique to single studies, 4 each replicated across 2 studies, and 3 each replicated across 3 studies.

Combined-study effect sizes for parameters which shared RTW subtask comparisons across more than one study showed that two parameters were consistent between STW and STS; these were: flexion-momentum time, and peak BCOM vertical velocity during rising. These parameters are both associated with the critical RTW event of seat-off. Flexion-momentum time reflects the transition from a stable base-of-support (BOS) in sitting to an unstable bipedal BOS at seat-off, whereas peak vertical BCOM velocity reflects the transfer of kinetic energy from a predominantly horizontal direction to a vertical one at seat-off [9].

Seat-off represents an event where risks to postural stability are high. For example, STS studies have confirmed that the vertical projection of the BCOM must be stabilised over a small BOS during the rising phase to mitigate the risk of falling due to a failure to stand up [60, 61]. It has also been established that the control of the BCOM horizontally before seat-off, and then vertically after seat-off, is relatively invariant at different STS speeds suggesting it is a tightly controlled and prioritised strategy [60]. During STW, prioritising stability around seat-off is equally crucial as it coincides with the cardinal tasks of STS and GI merging [11]. Therefore, the consistency in flexion-momentum time and peak vertical BCOM velocity between RTW tasks suggests that stability around seat-off is prioritised independently of how RTW is achieved.

The COP-BCOM horizontal distance, which is positively correlated with postural stability [27, 62], was also a consistent biomechanical parameter based on a combined-study effect size across two studies between STW and GI at toe-off. Toe-off proceeds seat-off in RTW and reflects a postural to dynamic phase transition in GI [63] where the base-of-support (BOS) changes from being bipedal to unipedal. It is possible therefore that postural stability is prioritised across RTW subtasks at events proceeding seat-off into GI.

In fact, biomechanical parameter consistency was observed into the first steps of walking after GI, at least in the single studies analysed. Specifically, step 1 stance width and velocity were consistent between STW and GI [27]. Furthermore, peak COP-BCOM distance during steps 1, 2, and 3 and the respective phase durations were consistent between STW and STSW [54]. It is possible these parameters are consistent (as defined) simply because events associated with steady-state walking are sufficiently dissociated from the initial transitional movement. If so, this would mean that these parameters are simply not influenced by any factors attributable to how RTW is performed. It would be interesting to determine whether parameters proceeding steady-state gait during deceleration phases and the transition to gait termination (GT) are influenced by RTW subtasks preceding them.

In other single-studies, consistency at seat-off in the anteroposterior position of both the BCOM and COP between STS and STW [11] was observed as was the peak vertical stance limb GRF [11], and the net GRF from both limbs [54], during rising which are practically coincident with seat-off [64]. Consistency was also observed in the time between movement-onset and peak GRFs in the anterior and posterior directions [55], in addition to the durations between movement-onset and the peak horizontal and vertical BCOM momenta (two events adjacent with seat-off) [11] and in the proportional time to

peak BCOM velocity [10]. However, as these data are based on single studies, caution in their interpretation should be exercised. That said, these parameters' apparent consistency between STS and STW around seat-off event supports the notion that control of stability might be prioritised around this unstable event.

It was surprising that the remaining single-study consistent parameter between STW and STS was in peak posterior (braking) GRF magnitude [55]. Braking GRFs are deployed to arrest the forward momentum generated during STS around seat-off and thereby achieve an upright position which is stable. They are typically higher in STS [10, 11] compared to STW because GI-onset occurs before upright is reached in STW and the maintenance of forward momentum after seat-off is desirable [16, 17]. The sample size these data were drawn from was small (n=8). So, it is possible that consistency (as defined) in peak posterior GRF between STW and STS was surprisingly found simply because the sample size was not large enough for true differences to be statistically significant.

### Limitations

### Sample sizes

All the included studies across RTW tasks possessed relatively low sample sizes. The maximum sample size in individual studies whose data were extracted was n=14 [56] and in pooled studies was n=31. Small sample sizes often lead to effect-size calculations being insufficiently precise [65] leading to poor confidence in the validity of the data rendering findings inconclusive. This is particularly pertinent in this review because it was forecasted that studies would not have a common effect size and not be functionally equivalent, so an *a priori* decision to apply random-effects modelling when calculating pooled effect sizes was made. However, pooled effect sizes were drawn from only a maximum of only 3 papers and a fixed-effect model was therefore employed due to the small number of studies because the estimate of the between-studies variance in a random-effects model would have poor precision in combined ES calculations [52].

### Number of combined studies

The small number of studies reviewed meant that synthesis of data was limited. Typically, if it is possible to extract and synthesise data to answer the literature review question, it must be conceded that interpretation of the synthesis will reflect bias if these data are drawn from a biased sample of published data [66]. The current literature review approached publication bias like many others by attempting to conduct as comprehensive a search as possible inclusive of the grey literature. Despite this, the risk remained that synthesised results would over-estimate true effect sizes [52] and an assessment of publication bias was planned. However, the numbers of included studies with common parameters was too small to perform this and subsequently, it was not practicable to use funnel plots because there was insufficient data available for them to be meaningful.

### Protocol characteristics

Instructing participants to move at self-selected tempo was the only selected protocol characteristic that was commonly adopted across all reviewed studies. During gait executed at self-selected velocity, step width and length parameters have been shown to be least variable, compared to slow and maximal velocities [67]. Adopting self-selected tempo in RTW is therefore advantageous because it allows participants to perform naturally and presumably safely, even if instructions to pause before walking is included in order to allow different variants of RTW to be investigated.

All other recorded protocol characteristics in reviewed studies were either unspecified or specified differently across studies. These characteristics included seat-height which was either explicitly stated or was 100% of knee-height (KH). Thus, the literature does not conclusively define a seat-height that both healthy and pathological participants can

execute RTW tasks safely and successfully from. Typical seat-heights of 100%KH present little difficulty for healthy participants. However, if a standardised protocol is to include participants with pathology e.g. stroke; a specified higher seat-height will be required between 115%KH [68] and 130%KH [69] as they are likely to find rising from 100%KH challenging [70]. One of the reviewed studies concluded that while a higher than normal seat-height (120%KH) required less effort compared to 100%KH, seat-height did not fundamentally alter the either STW or STSW task dynamics [54] and a higher seat-height is therefore desirable if a standardised protocol is to include participants with pathology.

### Gender representation

Gender was nor reported in 4 or the 9 studies reviewed, and in the 5 who did, only 2 studies included females. Gender and sex-specific differences in pathological processes exist including cardiovascular and neurological diseases [71], and in gait kinematics and muscle activity [72]. So, it is vital that interpretations of RTW data are not based on male data alone. As such, if clinical practice is to be informed, those data must be drawn equally from males and females, irrespective of whether sex and gender biases are intentional or not [73].

### Conclusions

This first of its kind systematic review confirmed our hypothesis that no published studies to date include an explicit aim to determine consistency in biomechanical parameters between RTW sub-tasks in healthy participants. The evidence synthesised from across the 9 eligible studies indicates that flexion-momentum time and peak BCOM vertical velocity during rising between STW and STS, and BCOM horizontal distance at initial toe-off between STW and GI are potentially consistent biomechanical parameters that do not vary significantly across RTW performance. Evidence from single studies revealed potentially 20 other consistent biomechanical parameters between RTW sub-tasks, particularly around the event of seat-off.

Seat-off represents a movement event associated with a high risk to postural stability in RTW. So, it is possible that parameter consistency was found here because postural stability is prioritised to mitigate risks of falling. Consistent parameters were also found after seat-off in GI and in the transition to walking, but it is unknown whether consistency observed here is simply a function of walking normalising downstream of RTW events. Nonetheless, this systematic review of the literature provides evidence supporting the notion that candidate consistent parameters might exist that could in theory discriminate and evaluate clinical change in the sensorimotor control of movement. Some of the parameters are based on temporal measures (e.g. flexion-momentum time) which means that clinical applications with patients performing RTW tasks using relatively low-tech equipment is certainly an aspiration if future work confirms parameters' consistency, validity, and reliability.

Any optimism associated with the evidence this systematic review provides needs to be cautious, however. Small sample sizes, inconsistent RTW protocols, and an underrepresentation of female gender limit the inferential nature of this evidence to a wider population. Therefore, while this systematic review suggests consistent biomechanical parameters across RTW subtasks exists, a specific evaluation of biomechanical parameters that remain consistent in a sample of both healthy male and female individuals between STW and STSW as the extremes of RTW is required.

### **CRediT Author Statement**

**Gareth D Jones:** Conceptualization, Methodology, Software, Formal Analysis, Investigation, Data Curation, Writing – Original Draft, Writing – Review and Editing, Visualization, Project Administration. **Gareth L Jones:** Formal Analysis, Investigation, Writing – Review and Editing **Darren C James:** Conceptualization, Methodology, Writing – Review and Editing, Visualization, Supervision. **Michael Thacker:** Conceptualization, Methodology, Writing – Review and Editing, Supervision. **David A Green:** Conceptualization, Methodology, Validation, Resources, Writing – Review and Editing, Project Administration, Supervision.

### Funding

The authors received no specific funding for this work.

### **Conflict of Interest Statement**

There are no conflicts of interest among any of the authors.

### References

[1] N. Hogan, D. Sternad, On rhythmic and discrete movements: reflections, definitions and implications for motor control, Exp Brain Res 181(1) (2007) 13-30. https://www.ncbi.nlm.nih.gov/pubmed/17530234.

 [2] T.A. Buckley, J.R. Oldham, B.A. Munkasy, K.M. Evans, Decreased Anticipatory Postural Adjustments During Gait Initiation Acutely Postconcussion, Arch. Phys. Med. Rehabil. 98(10) (2017) 1962-1968. https://www.ncbi.nlm.nih.gov/pubmed/28583462.

[3] A. Kerr, Rafferty, Hollands, Barber, Granat, A technique to record the sedentary to walk movement during free living mobility: A comparison of healthy and stroke populations, Gait Posture 52 (2017) 233-236. https://www.ncbi.nlm.nih.gov/pubmed/27940399.

[4] G.D. Jones, D.C. James, M. Thacker, D.A. Green, Sit-to-stand-and-walk from 120% Knee Height: A Novel Approach to Assess Dynamic Postural Control Independent of Lead-limb, Journal of visualized experiments : JoVE (114) (2016) e54323. https://www.ncbi.nlm.nih.gov/pubmed/27684456.

[5] M.E. Rogers, N.L. Rogers, N. Takeshima, M.M. Islam, Methods to assess and improve the physical parameters associated with fall risk in older adults, Prev. Med. 36(3) (2003) 255-64. https://www.ncbi.nlm.nih.gov/pubmed/12634016.

[6] K. Berg, S. Wood-Dauphine, J.I. Williams, D. Gayton, Measuring balance in the elderly: preliminary development of an instrument, Physiother. Can. 41(6) (1989) 304-311. https://utpjournals.press/doi/10.3138/ptc.41.6.304.

[7] G.E. Frykberg, B. Lindmark, H. Lanshammar, J. Borg, Correlation between clinical assessment and force plate measurement of postural control after stroke, J. Rehabil. Med. 39(6) (2007) 448-53. https://www.ncbi.nlm.nih.gov/pubmed/17624478.

[8] M. Schenkman, R.A. Berger, P.O. Riley, R.W. Mann, W.A. Hodge, Whole-body movements during rising to standing from sitting, Phys. Ther. 70(10) (1990) 638-48; discussion 648-51. https://www.ncbi.nlm.nih.gov/pubmed/2217543.

[9] P.O. Riley, M.L. Schenkman, R.W. Mann, W.A. Hodge, Mechanics of a constrained chair-rise, J Biomech 24(1) (1991) 77-85. https://www.ncbi.nlm.nih.gov/pubmed/2026635.

[10] M. Kouta, K. Shinkoda, N. Kanemura, Sit-to-Walk versus Sit-to-Stand or Gait Initiation: Biomechanical Analysis of Young Men, J Phys Ther Sci 18(2) (2006) 201-206. https://doi.org/10.1589/jpts.18.201.

[11] A. Magnan, B.J. McFadyen, G. St-Vincent, Modification of the sit-to-stand task with the addition of gait initiation, Gait Posture 4(3) (1996) 232-241. http://www.sciencedirect.com/science/article/pii/0966636295010483.

[12] Y. Breniere, M.C. Do, J. Sanchez, A Biomechanical Study Of The Gait Initiation Process, Journal De Biophysique & Medecine Nucleaire 5(4) (1981) 197-205. <Go to ISI>://WOS:A1981MV51500003.

[13] Y. Dessery, F. Barbier, C. Gillet, P. Corbeil, Does lower limb preference influence gait initiation?, Gait Posture 33(4) (2011) 550-5. https://www.ncbi.nlm.nih.gov/pubmed/21324699.

[14] I.N. Lyon, B.L. Day, Control of frontal plane body motion in human stepping,ExpBrainRes115(2)(1997)345-56.https://www.ncbi.nlm.nih.gov/pubmed/9224862.

[15] Y. Jian, D.A. Winter, M.G. Ishac, L. Gilchrist, Trajectory of the body COG and COP during initiation and termination of gait, Gait Posture 1(1) (1993) 9-22. http://www.sciencedirect.com/science/article/pii/0966636293900383.

[16] T. Buckley, C. Pitsikoulis, E. Barthelemy, C.J. Hass, Age impairs sit-to-walk motor performance, J Biomech 42(14) (2009) 2318-22. https://www.ncbi.nlm.nih.gov/pubmed/19656512.

[17] F. Malouin, B. McFadyen, L. Dion, C.L. Richards, A fluidity scale for evaluating the motor strategy of the rise-to-walk task after stroke, Clin. Rehabil. 17(6) (2003) 674-84. https://www.ncbi.nlm.nih.gov/pubmed/12971713.

[18] A. Kerr, B. Durward, K.M. Kerr, Defining phases for the sit-to-walk movement,Clin.Biomech.(Bristol, Avon)19(4)(2004)385-90.https://www.ncbi.nlm.nih.gov/pubmed/15109759.

[19] G.E. Frykberg, A.C. Aberg, K. Halvorsen, J. Borg, H. Hirschfeld, Temporal<br/>coordination of the sit-to-walk task in subjects with stroke and in controls, Arch.Phys.Med.Rehabil.90(6)(2009)1009-17.https://www.ncbi.nlm.nih.gov/pubmed/19480878.

[20] A. Kerr, V.P. Pomeroy, P.J. Rowe, P. Dall, D. Rafferty, Measuring movement fluency during the sit-to-walk task, Gait Posture 37(4) (2013) 598-602. https://www.ncbi.nlm.nih.gov/pubmed/23122898.

[21] M.L. Latash, The bliss (not the problem) of motor abundance (not redundancy), Exp Brain Res 217(1) (2012) 1-5. https://www.ncbi.nlm.nih.gov/pubmed/22246105.

[22] G. Schoner, Recent Developments and Problems in Human Movement Science and Their Conceptual Implications, Ecol. Psychol. 7(4) (1995) 291-314. <Go to ISI>://WOS:A1995UX22200005.

[23] E. Papi, P.J. Rowe, V.M. Pomeroy, Analysis of gait within the uncontrolled manifold hypothesis: stabilisation of the centre of mass during gait, J Biomech 48(2) (2015) 324-31. https://www.ncbi.nlm.nih.gov/pubmed/25488137.

[24] S.R. Lord, S.M. Murray, K. Chapman, B. Munro, A. Tiedemann, Sit-to-stand performance depends on sensation, speed, balance, and psychological status in addition to strength in older people, J. Gerontol. A Biol. Sci. Med. Sci. 57(8) (2002) M539-43. https://www.ncbi.nlm.nih.gov/pubmed/12145369.

[25] L. Dion, F. Malouin, B. McFadyen, C.L. Richards, Assessing mobility andlocomotor coordination after stroke with the rise-to-walk task, Neurorehabil.NeuralRepair17(2)(2003)https://www.ncbi.nlm.nih.gov/pubmed/12814053.

[26] S.E. Halliday, D.A. Winter, J.S. Frank, A.E. Patla, F. Prince, The initiation of gait in young, elderly, and Parkinson's disease subjects, Gait Posture 8(1) (1998) 8-14. https://www.ncbi.nlm.nih.gov/pubmed/10200394.

[27] T.A. Buckley, C. Pitsikoulis, C.J. Hass, Dynamic postural stability during sit-towalk transitions in Parkinson disease patients, Mov Disord 23(9) (2008) 1274-80. https://www.ncbi.nlm.nih.gov/pubmed/18464285.

[28] M. Martin, M. Shinberg, M. Kuchibhatla, L. Ray, J.J. Carollo, M.L. Schenkman, Gait initiation in community-dwelling adults with Parkinson disease: comparison with older and younger adults without the disease, Phys. Ther. 82(6) (2002) 566-77. https://www.ncbi.nlm.nih.gov/pubmed/12036398.

[29] A. Liberati, D.G. Altman, J. Tetzlaff, C. Mulrow, P.C. Gotzsche, J.P. Ioannidis, et al., The PRISMA statement for reporting systematic reviews and meta-analyses of studies that evaluate healthcare interventions: explanation and elaboration, BMJ 339 (2009) b2700. https://www.ncbi.nlm.nih.gov/pubmed/19622552.

[30] E.V. Villanueva, E.A. Burrows, P.A. Fennessy, M. Rajendran, J.N. Anderson, Improving question formulation for use in evidence appraisal in a tertiary care setting: a randomised controlled trial [ISRCTN66375463], BMC Med. Inform. Decis. Mak. 1 (2001) 4. https://www.ncbi.nlm.nih.gov/pubmed/11716797. [31] X. Huang, J. Lin, D. Demner-Fushman, Evaluation of PICO as a Knowledge Representation for Clinical Questions, AMIA Annual Symposium Proceedings 2006 (2006) 359-363. http://www.ncbi.nlm.nih.gov/pmc/articles/PMC1839740/.

[32] Centre for Reviews and Dissemination, Systematic Reviews: CRD's guidance for undertaking reviews in health care, University of York, York, 2009.

[33] D. Podsiadlo, S. Richardson, The timed "Up & Go": a test of basic functional mobility for frail elderly persons, J. Am. Geriatr. Soc. 39(2) (1991) 142-8. https://www.ncbi.nlm.nih.gov/pubmed/1991946.

[34] A. Paez, Gray literature: An important resource in systematic reviews, J. Evid.BasedMed.10(3)(2017)233-240.https://www.ncbi.nlm.nih.gov/pubmed/28857505.

[35] A. Bayer, W. Tadd, Unjustified exclusion of elderly people from studies submitted to research ethics committee for approval: descriptive study, BMJ 321(7267) (2000) 992-3. https://www.ncbi.nlm.nih.gov/pubmed/11039965.

[36] C. Itoh, T. Kasai, S. Wakayama, Comparison of forward and backward walking in gait initiation, Physiotherapy 101 (2015) e660. http://www.sciencedirect.com/science/article/pii/S0031940615035300.

[37] T. Gelat, A. Le Pellec, Why anticipatory postural adjustments in gait initiation need to be modified when stepping up onto a new level?, Neurosci Lett 429(1) (2007) 17-21. https://www.ncbi.nlm.nih.gov/pubmed/17964073.

[38] F. Allali, S. El Aichaoui, H. Khazani, B. Benyahia, B. Saoud, S. El Kabbaj, et al., High prevalence of hypovitaminosis D in Morocco: relationship to lifestyle, physical performance, bone markers, and bone mineral density, Semin. Arthritis Rheum. 38(6) (2009) 444-51. https://www.ncbi.nlm.nih.gov/pubmed/18336870.

[39] S. Adamson, R. Lorimer, J.N. Cobley, R. Lloyd, J. Babraj, High intensity training improves health and physical function in middle aged adults, Biology (Basel) 3(2) (2014) 333-44. https://www.ncbi.nlm.nih.gov/pubmed/24833513.

[40] D. Vervoort, N. Vuillerme, N. Kosse, T. Hortobagyi, C.J. Lamoth, Multivariate Analyses and Classification of Inertial Sensor Data to Identify Aging Effects on the Timed-Up-and-Go Test, PLoS One 11(6) (2016) e0155984. https://www.ncbi.nlm.nih.gov/pubmed/27271994.

[41] Centre for Evidence-Based Physiotherapy, PEDro scale. http://www.pedro.org.au/english/downloads/pedro-scale/, 1999 (accessed December 29th 2012)).

[42] C.G. Maher, C. Sherrington, R.D. Herbert, A.M. Moseley, M. Elkins, Reliability of the PEDro scale for rating quality of randomized controlled trials, Phys. Ther. 83(8) (2003) 713-21. https://www.ncbi.nlm.nih.gov/pubmed/12882612.

[43] S. Moola, Z. Munn, C. Tufanaru, E. Aromataris, K. Sears, R. Sfetcu, et al., Chapter 7: Systematic reviews of etiology and risk, in: E. Aromataris, Z. Munn (Eds.), JBI Manual for Evidence Synthesis, The Joanna Briggs Institute, Adelaide, Australia, 2020.

[44] E. Aromataris, Z. Munn, (Editors), JBI Manual for Evidence Synthesis. https://synthesismanual.jbi.global.

https://doi.org/10.46658/JBIMES-20-01, 2020 (accessed 27 July 2020).

[45] Z. Jordan, Z. Munn, E. Aromataris, C. Lockwood, Now that we're here, where are we? The JBI approach to evidence-based healthcare 20 years on, International journal of evidence-based healthcare 13(3) (2015) 117-20. https://www.ncbi.nlm.nih.gov/pubmed/26154180.

[46] J. Cohen, A Coefficient of Agreement for Nominal Scales, Educ. Psychol. Meas. 20(1) (2016) 37-46. <Go to ISI>://WOS:A1960CCC3600004.

[47] J.R. Landis, G.G. Koch, The measurement of observer agreement for categorical data, Biometrics 33(1) (1977) 159-74. https://www.ncbi.nlm.nih.gov/pubmed/843571.

[48] A. Franco, M.N. de Oliveira, M.T. Campos Vidigal, C. Blumenberg, A.A. Pinheiro, L.R. Paranhos, Assessment of dental age estimation methods applied to brazilian children - a systematic review and meta-analysis, Dentomaxillofac. Radiol. (2020) 20200128. https://www.ncbi.nlm.nih.gov/pubmed/32479117.

[49] J. Cohen, Statistical power analysis for the behavioral sciences, Second ed., Academic Press, New York, 1988.

[50] L.V. Hedges, Distribution Theory for Glass's Estimator of Effect Size and Related Estimators, Journal of Educational Statistics 6(2) (1981) 107-128. http://www.jstor.org/stable/1164588.

[51] S. Nakagawa, I.C. Cuthill, Effect size, confidence interval and statistical significance: a practical guide for biologists, Biol. Rev. Camb. Philos. Soc. 82(4) (2007) 591-605. https://www.ncbi.nlm.nih.gov/pubmed/17944619.

[52] M. Borenstein, L.V. Hedges, H.J. P.T., H.R. Rothstein, Introduction to Meta-Analysis, John Wiley and Sons Ltd., Chichester, UK, 2009.

[53] L. Hedges, I. Olkin, Statistical Methods for Meta-Analysis, Academic Press, New York, NY, 1985.

[54] G.D. Jones, D.C. James, M. Thacker, E.J. Jones, D.A. Green, Sit-to-walk and sitto-stand-and-walk task dynamics are maintained during rising at an elevated seatheight independent of lead-limb in healthy individuals, Gait Posture 48 (2016) 226-229. https://www.ncbi.nlm.nih.gov/pubmed/27336849.

[55] A. Kerr, K. Kerr, Differences in the Initial Propulsive Force Between Sit to Walk and Sit to Stand in Healthy Subjects, Physiotherapy 87(2) (2001) 87. http://www.sciencedirect.com/science/article/pii/S0031940605604518. [56] A. Kerr, K.M. Kerr, Sit-to-Stand and Sit-to-Walk, Physiotherapy 88(7) (2002) 437. https://doi.org/10.1016/S0031-9406(05)61283-7.

[57] S. Mezzarobba, M. Grassi, R. Valentini, P. Bernardis, Postural control deficit during sit-to-walk in patients with Parkinson's disease and freezing of gait, Gait Posture 61 (2018) 325-330. https://www.ncbi.nlm.nih.gov/pubmed/29413805.

[58] F.C.d. Silva, A.M. Rodrigues, M.J. Wiest, Effects of a subsequent task after sitto-stand movement on muscle activation and initiation of movement, Rev Bras Cineantropom Desempenho Hum 15(4) (2013) 458-466. https://dx.doi.org/10.5007/1980-0037.2013v15n4p458.

[59] R.J. Light, J.D. Singer, J.B. Willett, The visual presentation and interpretation of meta-analyses, The handbook of research synthesis., Russell Sage Foundation, New York, NY, US, 1994, pp. 439-453.

[60] Y.C. Pai, M.W. Rogers, Control of body mass transfer as a function of speed of ascent in sit-to-stand, Med. Sci. Sports Exerc. 22(3) (1990) 378-84. https://www.ncbi.nlm.nih.gov/pubmed/2381306.

[61] Y.C. Pai, M.W. Rogers, Segmental contributions to total body momentum in sit-to-stand, Med. Sci. Sports Exerc. 23(2) (1991) 225-30. https://www.ncbi.nlm.nih.gov/pubmed/2017019.

[62] C.J. Hass, D.E. Waddell, R.P. Fleming, J.L. Juncos, R.J. Gregor, Gait initiation and dynamic balance control in Parkinson's disease, Arch. Phys. Med. Rehabil. 86(11) (2005) 2172-6. https://www.ncbi.nlm.nih.gov/pubmed/16271566.

[63] Y. Breniere, M. Cuong Do, S. Bouisset, Are dynamic phenomena prior to stepping essential to walking?, J Mot Behav 19(1) (1987) 62-76. https://www.ncbi.nlm.nih.gov/pubmed/23944913.

[64] C.A. McGibbon, D. Goldvasser, D.E. Krebs, D. Moxley Scarborough, Instant of chair-rise lift-off can be predicted by foot-floor reaction forces, Hum Mov Sci 23(2) (2004) 121-32. https://www.ncbi.nlm.nih.gov/pubmed/15474173.

[65] E. Prashanti, K.N. Sumanth, P. Renjith George, L. Karanth, H.H. Soe, Management of gag reflex for patients undergoing dental treatment, Cochrane Database Syst. Rev. (10) (2015) CD011116. https://www.ncbi.nlm.nih.gov/pubmed/26423025.

[66] J.A. Sterne, M. Egger, G.D. Smith, Systematic reviews in health care: Investigating and dealing with publication and other biases in meta-analysis, BMJ 323(7304) (2001) 101-5. https://www.ncbi.nlm.nih.gov/pubmed/11451790.

[67] N. Sekiya, H. Nagasaki, H. Ito, T. Furuna, Optimal walking in terms of variability in step length, J. Orthop. Sports Phys. Ther. 26(5) (1997) 266-72. https://www.ncbi.nlm.nih.gov/pubmed/9353690. [68] M.W. Rodosky, T.P. Andriacchi, G.B. Andersson, The influence of chair height on lower limb mechanics during rising, J. Orthop. Res. 7(2) (1989) 266-71. https://www.ncbi.nlm.nih.gov/pubmed/2918425.

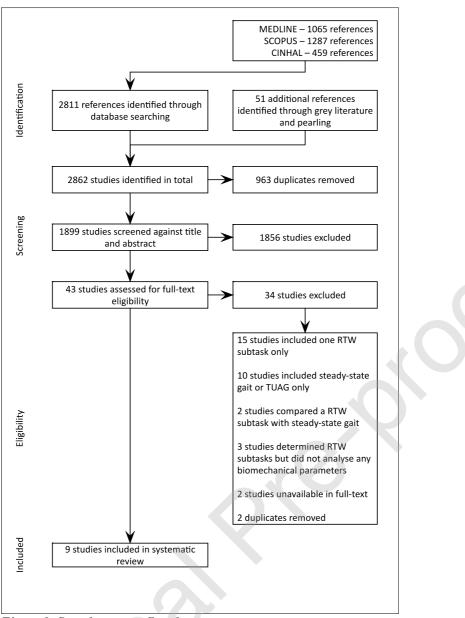
[69] S. Rocha Ade, R.J. Knabben, S.M. Michaelsen, Non-paretic lower limb constraint with a step decreases the asymmetry of vertical forces during sit-to-stand at two seat heights in subjects with hemiparesis, Gait Posture 32(4) (2010) 457-63. https://www.ncbi.nlm.nih.gov/pubmed/20674364.

[70] G. Roy, S. Nadeau, D. Gravel, F. Malouin, B.J. McFadyen, F. Piotte, The effect of foot position and chair height on the asymmetry of vertical forces during sit-to-stand and stand-to-sit tasks in individuals with hemiparesis, Clin. Biomech. (Bristol, Avon) 21(6) (2006) 585-93. https://www.ncbi.nlm.nih.gov/pubmed/16540217.

[71] V. Regitz-Zagrosek, Sex and gender differences in health. Science & Society Series on Sex and Science, EMBO Rep 13(7) (2012) 596-603. https://www.ncbi.nlm.nih.gov/pubmed/22699937.

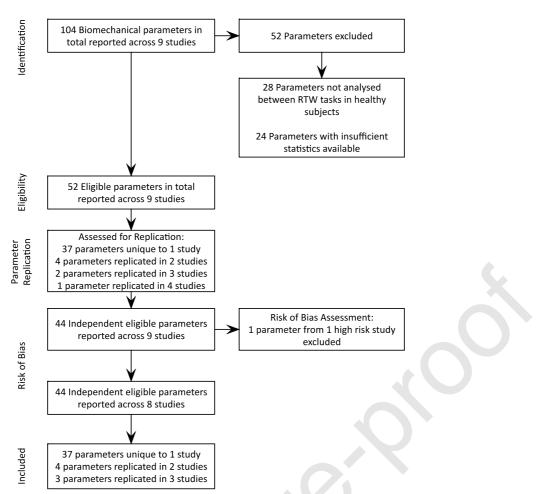
[72] E.S. Chumanov, C. Wall-Scheffler, B.C. Heiderscheit, Gender differences in walking and running on level and inclined surfaces, Clin. Biomech. (Bristol, Avon) 23(10) (2008) 1260-8. https://www.ncbi.nlm.nih.gov/pubmed/18774631.

[73] C. Pritlove, C. Juando-Prats, K. Ala-Leppilampi, J.A. Parsons, The good, the bad, and the ugly of implicit bias, Lancet 393(10171) (2019) 502-504. https://www.ncbi.nlm.nih.gov/pubmed/30739671.



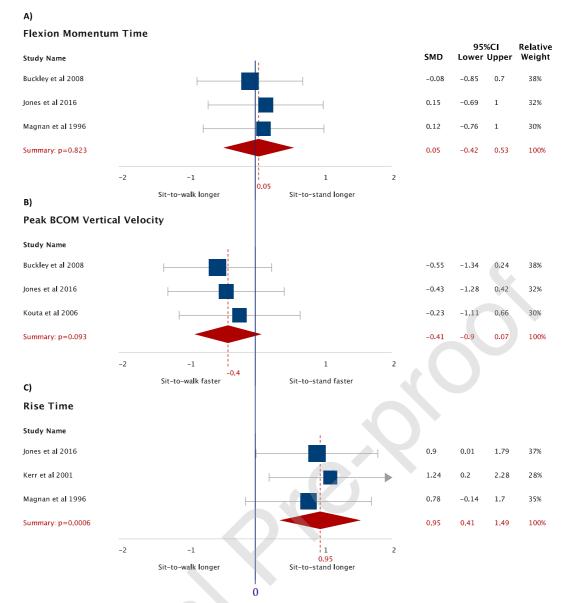
*Figure 1: Search strategy flowchart The strategy follows PRISMA guidelines for preferred reporting of systematic reviews [20]* 

### **Journal Pre-proof**



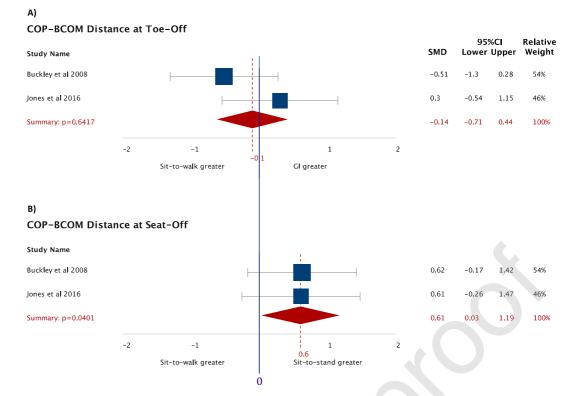
*Figure 2: Final Biomechanical Parameter Inclusion Flowchart Flow from total number of biomechanical parameters measured in the 7 reviewed studies, to parameter data eventually extracted after assessing for eligibility, replication, and risk of bias* 

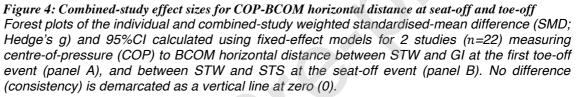
### Journal Pre-proof



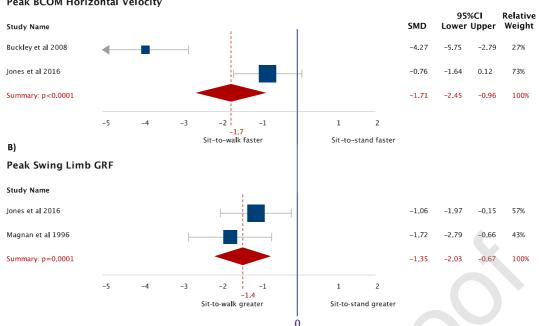
### Figure 3: Combined-study effect sizes for parameters shared in 3 studies

Forest plots of the individual and combined-study weighted standardised-mean difference (SMD; Hedge's g) and 95%Cls calculated using fixed-effect models for 3 studies (n=31) measuring flexion-momentum time (movement-onset to seat-off) between STW and STS (panelA), 3 studies (n=31) measuring peak BCOM vertical velocity during rising between STW and STS (panel B) and 3 studies (n=27) measuring rise-time (movement-onset to upright) between STW and STS (panel STS (panel C). No difference (consistency) is demarcated as a vertical line at zero (0).

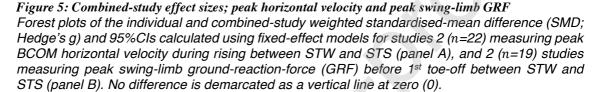




24



### A) Peak BCOM Horizontal Velocity



### ournal Pre-proof

Table 1: Included Studies' Participant and Protocol Characteristics Included studies are listed with their aims by first author alphabetically showing; number of participants, gender, and mean (±SD) participant age, dominant limb, mass, plus walking distance and number of trials per RTW task.

All Studies	Silva <i>et al</i> 2013	Mezzarobba <i>et</i> <i>al</i> 2018	Magnan <i>et al</i> 1996	Kouta <i>et al</i> 2006	Kerr <i>et al</i> 2004	Kerr & Kerr 2002	Kerr & Kerr 2001	Jones <i>et al</i> 2016	Buckley <i>et al</i> 2008	Study Aim(s)	
	To determine if the central nervous system requires longer to process information during STW (with the inclusion of a new task of GI) compared to STS by assessing anticipatory activation of muscle onset latencies in young healthy participants	To determine if there are differences in postural control between progressively complex Mezzarobba <i>et</i> motor tasks (walking, GI, and STW) within participants with PD (±FOG) or age-matched <i>al</i> 2018 healthy participants and thereby assess if PD motor profiles can be differentiated between those with, and without FOG	To determine how kinetic and spatial-temporal parameters during STS are modified with the additional task of gait-initiation during STW in young healthy male participants	To determine if there are differences in temporal parameters during GI compared to STW and in peak horizontal and vertical velocities of the head-arms-trunk segment during STS compared to STW in young healthy male participants	To determine discrete phases of STW movement (based on phases previously described during STS, and on events described during STW) and then assess the repeatability of the determined STW phases in healthy participants.	Kerr & Kerr To determine if there is a difference in the initial flexion momentum phase duration 2002 during STS compared to STW in healthy participants	Kerr & Kerr To determine if there are larger initial propulsive forces during STS compared to STW 2001 in young healthy participants	Jones <i>et al</i> To determine if seat-height or limb-lead influence temporal and kinetic task dynamics 2016 either during STW or STSW in young healthy participants	Buckley <i>et al</i> To determine if performance of the component STW tasks (STS and GI) are modified 2008 during STW in people with PD compared to age-matched healthy participants	Aim(s)	
66	12	12	9*	9	13	14	8	10	12	п	
79%	12	6	10	9	NR	NR	NR	ъ	NR	R	Gender (n)
21%	0	0	0	0	NR	NR	NR	ъ	NR	п	) der
39.6 (16.30)	24.5 (3.70)	67.4 (8.70)	28.0 (6.00)	21.8 (2.50)	39.8 (12.30)	39.8 (11.80)	43.4 32-56†	29.1 (7.70)	63.0 (6.93)	Mean (SD)	Age (yrs)
I	NR	NR	NR	NR	NR	NR	NR	9	NR	Righ	Dor
I	NR	NR	NR	NR	NR	NR	NR	-	NR	Right Left	Dom Leg ( <i>n</i> )
1.725 (0.071)	1.720 (0.040) 70.92	NR NR	1.760 (0.050) 74.60	1.703 (0.049) 65.10 (6.80)	1.760 (0.100) 80.90 (15.80)	1.760 (0.11)	NR NR	1.710 (0.077) 73.50	1.698 (0.100) 79.20 (15.59)	$\leq$	Height (m)
1) 74.04	0) 70.	24.	0) 74.	9) 65.	0) 80.	(0.110) 80.90	_	7) 73.	0) 79.	Me	-
04 (10.72)	92 (3.85)	24.9‡ (3.9‡)	.60 (11.40)	10 (6.80)	90 (15.80)	90 (15.80)	NR NR	50 (10.90)	20 (15.59)		Mass (kg)
I	I	10	σī	ω	7	NR	NR	ъ	4	(m)	Walk Distance
		ப	NR	NR	ъ	5	з	б	ъ	( <i>n</i> )	Task Trials

DOM – dominant; F – female; FOG – freezing-of-gait; GI – gait-initiation; M – male; NR - data "not reported"; PD – Parkinson's disease; STW – sit-to-stand; STW – sit-to-walk; STSW – sit-to-stand-and-walk; \*Data analysed in this study based on n=9; †data refers to age range; ‡data refers to Body Mass Index (BMI) in kg/m<sup>2</sup>

### **Journal Pre-proof**

# Table 2: Included Studies' Protocol Constraint Characteristics and RTW Task Comparisons Experimental protocol details with respect to movement tasks and within-study parameters

s' Protocol Cons. Jetails with resp	Table 2: Included Studies' Protocol Constraint Characteristics and RTW Task Comparisons Experimental protocol details with respect to movement tasks and within-study param	cs and RTW Ta tasks and withi	sk Compari n-study pa	sons rameters				
Feet Position	Seat Height (%KH)	Seat Height (m)	Knee Angle (°)	Arm use	Tempo	Ecological Task	Lead Limb	RTW Subtask Comparisons
SS then maintained	NR	NR	105	Constrained to trunk	SS	Target or Object	SS then maintained	GI v STS v STW
Standardised	100 & 120	I	I	NR	SS	UL Task	Dom and NonDom	STW v STSW
Parallel	I	0.45	I	NR	SS	NR	SS then maintained	STS v STW
Kept Constant	100	I	1	Constrained to trunk	SS	NR	NR	STS v STW
Parallel	100	Ι		Constrained to trunk	SS	NR	SS then maintained	STS v STW
Shoulder Width Apart	100	1	90	NR	SS	NR	NR	GI v STS v STW
	100	1	Ι	Constrained to trunk	SS	NR	SS then maintained	STS v STW
	100	I	100	Constrained to waist	SS	NR	Left	GI v STW
SS then maintained	001					NR	NR	
	ol details with resp Feet Position SS then maintained Standardised Parallel Parallel Parallel Parallel Parallel	Jetails with respect to movement         st Position       Seat Height (%KH)         then       NR         ntained       100 & 120         ndardised       100 & 120         allel       -         ot Constant       100         allel       100         allel       100         allel       100	Jetails with respect to movement tasks and within and within them       Seat Height (%KH)       Seat Height (m)         attem       NR       NR       NR         ntained       100 & 120       -         ndardised       100 & 120       -         allel       -       0.45         ot Constant       100       -         allel       100       -         allel       100       -	Jetails with respect to movement tasks and within-study part for the seat Height (%KH)       Seat Height (%KH)       Seat Height (m)       Knee Angle angle then the seat Height (m)       Knee Angle angle the seat Height (m)       Knee Angle angle angle angle and the seat Height (m)       Knee Angle	Arm use Arm use Instrained to trunk NR NR NR Instrained to trunk NR	Arm use     Trained to trunk       NR     NR       NR     NR       Nrained to trunk     Instrained to trunk	Arm useTempoEcological Tasknstrained to trunkSSTarget or ObjectNRSSUL TaskNRSSNRnstrained to trunkSSNRNRSSNRNRSSNRNRSSNRNRSSNRNRSSNRNRSSNR	Arm useTempoEcological Tasknstrained to trunkSSTarget or ObjectNRSSUL TaskNRSSNRnstrained to trunkSSNRNRSSNRNRSSNRNRSSNRNRSSNRNRSSNRNRSSNR

### Table 3: Risk of Bias Within Studies

Consensus data are presented per quality domain for each paper with the inter-rater agreement shown as the  $\kappa$  statistic

									-
Study	1. Inclusion criteria	2. Subject description	3. Exposure measurement	4. Condition Measurement	5. Confounders identified	6. Confounders managed	7. Outcome measurement	8. Statistical analyses	Overall Bias
Buckley et al 2008	0	1	0	0	0	0	0	0	1
Jones et al 2016	1	0	0	0	1	0	0	0	2
Kerr & Kerr 2001	1	1	0	0	2	1	1	0	6
Kerr & Kerr 2002	1	2	2	0	2	1	2	2	12
Kerr et al 2004	0	1	0	0	0	0	0	0	1
Kouta et al 2006	1	0	0	0	1	0	0	0	2
Magnan et al 1996	1	0	0	0	0	0	0	0	1
Mezzarobba et al 2018	0	0	0	0	0	0	0	0	0
Silva et al 2013	1	1	1	0	0	2	0	0	5
$\kappa$ statistic	0.73	0.44	1.00	1.00	0.80	0.49	0.31	1.00	0.772

Risk of Bias Assessment Criteria

Scoring Code: 0 – Low bias; 1 – Unclear; 2 – High Bias

### ournal Pre-proo

effect-size 95%Cl includes the null value – the zero effect line. for each study with studies listed in alphabetical order; parameters are described showing the RTW subtask comparison, the parameter type, measurement units with respect to movement event(s) associated with the respective parameter, and whether the parameter is consistent between the RTW subtasks (i.e. when the Table 4: Effect sizes in biomechanical parameters unique to 1 study Mean (SD) data for each RTW subtask are shown per biomechanical parameter with 95%Cl around the effect-size g (Hedge's g). Individual parameters are shown

Jones <i>et</i> al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Buckley et al 2008	Buckley et al 2008	Buckley et al 2008	Buckley et al 2008	Buckley <i>et al</i> 2008	Study	
14 Distance_Max COP-BCOM_Step3 (STS(W)* vs STW)	13 Time_Step2 (STS(W)* vs STW)	12 Distance Max COP-BCOM_Step2 (STS(W)* vs STW)	11 Time_Step1 (STS(W)* vs STW)	10 Distance_Max COP-BCOM_Step1 (STS(W)* vs STW)	9 Time_GI-Onset to Swing Toe-off (GI Time) (STS(W)* vs STW)	8 Distance_COP-BCOM_at GI-Onset (STS(W)* vs STW)	7 Distance_COP-BCOM_at Upright (STS(W*) vs STW)		5 Velocity_BCOM_Horizontal at Seat-off (STS vs STW)	4 Distance_COP-BCOM_at Initial-Contact (GI vs STW)	3 Distance_FirstStep Width (GI vs STW)	2 Velocity_FirstStep Vel (GI vs STW)	1 Distance_Step Length (GI vs STW)	Parameter	
Max Dist Between Events (m)	Time Between Events (s)	Max Dist Between Event (m)	Time Between Events (s)	Max Dist Between Events (m)	Time Between Events (s)	Distance at Event (m)	Distance at Event (m)	Max Force Between Movt-Onset Events (%BW)	Velocity at Event (m.s <sup>-1</sup> )	Distance at Event (m)	Distance Between Events (m)	Mean Velocity Between Events (m.s <sup>-1</sup> )	Distance Between Events (m)	Parameter Type (Units)	
Initial-contact2 (2 <sup>nd</sup> )	Initial-contact	Initial-contact	Toe-off	Toe-off	GI-onset	GI-onset	Upright	Movt-Onset	Seat-off	Initial-contact	Heel-off	Heel-off	Heel-off	Event 1	
Initial-contact3 (3 <sup>rd</sup> )	Initial-contact2 (2 <sup>nd</sup> )	Initial-contact2 (2 <sup>nd</sup> )	Initial-contact	Initial-contact	Toe-off	I	I	Seat-off	I	l	Initial-contact	Initial-contact	Initial-contact	Event 2	
1	1	1	1	I	I	I I	1	-	-	0.281 (0.037)	0.241 (0.065)	0.940 (0.173)	0.528 (0.048)	GI GI Mean (SD)	
0.260 (0.032)	0.620 (0.063)	0.230 (0.032)	0.440 (0.063)	0.250 (0.032)	0.610 (0.095)	0.020 (0.013)	0.020 (0.000)	130.0 (0.095)	0.440 (0.069)	1	-	1	1	STS STS Mean (SD)	
0.260 (0.032)	0.580 (0.063)	0.230 (0.032)	0.400 (0.063)	0.260 (0.032)	0.460 (0.095)	0.050 (0.032)	0.140 (0.032)	136.0 (0.095)	0.510 (0.069)	0.337 (0.034)	0.282 (0.062)	1.080 (0.173)	0.581 (0.056)	STW STW Mean (SD)	
0.000	0.607	0.000	0.607	-0.304	1.518	-1.196	-5.152	-0.607	-0.977	-1.539	-0.622	-0.782	-0.987	g	
(-0.841 to 0.841)	(-0.257 to 1.472)	(-0.841 to 0.841)	(-0.257 to 1.472)	(-1.151 to 0.544)	(0.541 to 2.495)	(-2.124 to -0.268)	(-7.034 to -3.270)	(-1.472 to 0.257)	(-1.803 to -0.151)	(-2.436 to -0.641) 0.001	-0.622 (-1.417 to 0.173)	-0.782 (-1.589 to 0.026)	-0.987 (-1.814 to -0.160)	(95%CI)	
1.000	0.169	1.000	0.169	0.483	0.002	0.012	0.000	0.169	0.020	0.001	0.125	0.058	0.019	q	
Y	Y	Y	Y	Y	z	N	z	Y	Z	N	Y	Y	z	Cons	

### nna

Kouta <i>et</i> al 2006	Kouta et al 2006	Kouta <i>et</i> al 2006	Kouta <i>et</i> al 2006	Kouta <i>et</i> al 2006	Kouta <i>et</i> al 2006	Kouta <i>et</i> al 2006	Kerr et al 2004	Kerr & Kerr 2001	Kerr & Kerr 2001	Kerr & Kerr 2001	Kerr & Kerr 2001	Jones <i>et</i> <i>al</i> 2016	Jones <i>et</i> al 2016	Jones et al 2016	Study
29 Velocity_Peak HAT_Horizontal before Seat-off (STS vs STW)	28 Velocity_BCOM_Horizontal at Peak BCOM Vertical (STS vs STW)	27 Distance_Total BCOM Displacement_Vertical (STS vs STW)	26 Distance_Total BCOM Displacement_Horizontal (STS vs STW)	25 Time%_Peak Swing GRF Vert to Swing Toe-off (GI vs STW)	24 Time%_Movt-Onset to Peak BCOM 24 Vel_Vertical (STS vs STW)	23 Time%_Movt-Onset to Peak HAT Vel_Horizontal (STS vs STW)	22 Force_PeakGRF_Mediolateral (STS vs STW)	21 Time_Movt-Onset to PeakGRF_Posterior (STS vs STW)	20 Time_Movt-Onset to PeakGRF_Anterior (STS vs STW)	19 Force_PeakGRF_Anterior (Propulsive) (STS vs STW)	18 Force_PeakGRF_Posterior (Braking) (STS vs STW)	17 Time_Go-Signal to Step3 (Overall Task Time) (STS(W)* vs STW)	16 Time_Movt-Onset to Step3 (Overall Movt Time) (STS(W)* vs STW)	15 Time_Step3 (STS(W)* vs STW)	Parameter
Maximum Velocity Between Events (m.s <sup>-1</sup> )	Velocity at Event (m.s <sup>-1</sup> )	Distance Between Events (% of Height)	Distance Between Events (% of Height)	Proportional Time Between Events (%Total Time)	Proportional Time Between Events (%Total Time)	Proportional Time Between Events (%Total Time)	Maximum Force Between Events (%BW)	Time Between Events (%Total Time)	Time Between Events (%Total Time)	Maximum Force Between Events (%BW)	Maximum Force Between Events (%BW)	Time Between Events (s)	Time Between Events (s)	Time Between Events (s)	Parameter Type (Units)
Movt-Onset	Peak BCOM Vertical Velocity	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Go-signal	Movt-Onset	Initial-contact2 (2 <sup>nd</sup> )	Event 1
Seat-off	V	Upright	Upright	Toe-off	Peak BCOM Vel_Vertical	Peak HAT vel _Horizontal	Seat-off	PeakGRF_ Posterior	PeakGRF_ Anterior	Upright or Toe- off	Upright or Toe- off	Initial-contact3 (3 <sup>rd</sup> )	Initial-contact3 (3 <sup>rd</sup> )	Initial-contact3 (3 <sup>rd</sup> )	Event 2
1		1	I	54.900 (10.200)	1	1	1							 	GI GI Mean (SD)
0.620 (0.090)	0.160 (0.060)	0.167 (0.015)	0.183 (0.025)	1	67.900 (6.300)	37.700 (2.400)	4.400 (0.580)	43.300 (3.000)	30.040 (9.040)	0.260 (0.760)	11.370 (2.130)	4.970 (0.569)	4.550 (0.569)	0.580 (0.032)	STS STS Mean (SD)
0.720 (0.110)	0.370 (0.180)	0.159 (0.014)	0.329 (0.151)	65.400 (10.100)	66.600 (3.000)	41.500 (4.800)	7.900 (0.985)	43.120 (5.620)	35.780 (6.600)	1.430 (1.260)	13.320 (3.620)	3.050 (0.285)	2.700 (0.253)	0.560 (0.032)	STW STW Mean (SD)
-0.950	-1.495	0.527	-1.289	-0.988	0.252	-0.957	-4.199	0.038	-0.688	-1.067	-0.623	4.096	4.032	0.607	Ø
(-1.893 to -0.008)	(-2.519 to -0.472)	(-0.375 to 1.428)	(-2.278 to -0.300)	(-1.935 to -0.041)	(-0.635 to 1.139)	(-1.899 to -0.014)	(-5.601 to -2.797)	(-0.892 to 0.968)	(-1.653 to 0.276)	(-2.078 to -0.057)	(-1.582 to 0.335)	(2.515 to 5.677)	(2.469 to 5.59)	(-0.257 to 1.472)	(95%Cl)
0.048	0.004	0.252	0.011	0.041	0.578	0.047	0.000	0.936	0.162	0.038	0.202	0.000	0.000	0.169	q
Z	Ν	Y	Z	z	Y	Z	Z	Y	Y	z	Y	N	Ν	Υ	Cons

(m.s<sup>-1</sup>)

### ournal Pre-proof

1996	Magnan et al	Magnan <i>et al</i> 1996	Magnan <i>et al</i> 1996	Magnan <i>et al</i> 1996	Magnan <i>et al</i> 1996	Magnan <i>et al</i> 1996	Magnan <i>et al</i> 1996	Kouta <i>et</i> al 2006	Study
(oro consistent normatical (%BW) Vertical	37 Force_Stance-Limb PeakGRF_Vertical	$_{36}$ Position_COP_AP_at Seat-off (STS vs STW)	35 Position_BCOM_AP_at Seat-off (STS vs STW)	$\frac{34}{vsSTW} Peak BCOM_Vertical \ (STS$	33 Momentum_Peak BCOM_Horizontal (STS vs STW)	32 Time_Movt-Onset to Peak BCOM Momentum_Vertical (STS vs STW)	31 Time_Movt-Onset to Peak BCOM Momentum_Horizontal (STS vs STW)	<sup>7</sup> 30 Force_Stance-Limb PeakGRF_Vertical (GI Between Events vs STW) (%BW)	Parameter
(%BW)	Maximum Force Between Events	Position at Event (m) AP direction	Position at Event (m) AP direction	Max Momentum Between Events (kg.m.s <sup>-1</sup> )	Max Momentum Between Events (kg.m.s <sup>-1</sup> )	Time Between Events (s)	Time Between Events (s)	Maximum Force Between Events (%BW)	Parameter Type (Units)
2. Distance and	Movt-Onset	Seat-off	Seat-off	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Movt-Onset	Event 1
Vertical	Peak BCOM Momentum	I		Upright	Upright	Peak BCOM Momentum Vertical	Peak BCOM Momentum Horizontal	Initial-contact	Event 2
	1		1					115.300 (4.100)	GI GI Mean (SD)
own where to a	59.260 (3.950)	0.026 (0.023)	-0.014 (0.035)	47.700 (6.800)	39.100 (6.000)	1.110 (0.170)	0.680 (0.120)		STS STS Mean (SD)
	57.300 (3.790) 0.484	0.024 (0.031) 0.070	-0.012 (0.028) -0.060	53.800 (8.300)	47.800 (7.400)	1.020 (0.160) 0.521	0.620 (2.110) 0.038	108.200 (7.100) 1.170	STW STW Mean (SD)
	0.484	0.070	-0.060	-0.768	-1.234	0.521	0.038	1.170	g
	(-0.415 to 1.382)	(-0.813 to 0.953)	(-0.943 to 0.823)	(-1.960 to 0.154)	-1.234 (-2.214 to -0.253) 0.014	(-0.380 to 1.422)	(-0.844 to 0.921)	(0.199 to 2.141)	(95%CI)
:	0.291	0.877	0.894	0.102	0.014	0.257	0.932	0.018	q
	Y	Y	Y	Y	Z	Y	Y	Z	Cons

GRF – ground-reaction-force; Max – maximum; Momentum – refers to a momentum measurement parameter; Movt – movement; NR – data "not reported"; Position – refers to a position in a certain direction measurement parameter; STS – sit-to-stand; STS(W) – sit-to-stand-and-walk; STW – sit-to-walk; Time – refers to a time-related measurement parameter; vel – velocity; Velocity – refers to a velocity measurement parameter; vert – velocity; Velocity – refers to a data from STSW analogous to STS simum; trx... S(W) – sit-to-stand-atu-

### ournal Pre-proof

## Table 5: Summary of all consistent kinematic and kinetic biomechanical parameters

which cross the line of zero-effect RTW subtask comparisons of parameters with their respective RTW phase or event are shown with single-study (g) and combined (M) effect-sizes and 95%Cls

23 W	22 W	21 W	20 W	19 W	18 W	17 W	16 W	15 G	14 R	13 R		11 R	10 R		9 R		8 R	7 R	6 R	5 R	4 R	3 R	2 R		1 R	No. P
Walking /Step3	Walking /Step3	Walking /Step2	Walking /Step2	Walking /Step1	Walking /Step1	Walking /Step1	Walking/Step1	GI/Toe-off	Rising	Rising	Rising	Rising	Rising		Rising		Rising/Seat-off	Rising/Seat-off	Rising	Rising	Rising	Rising	Rising		Rising	Phase/Event
Time_Step3	Distance_Max COP-BCOM_Step3	Time_Step2	Distance_Max COP-BCOM_Step2	Velocity_FirstStepBCOM Velocity	Distance_FirstStep Width	Time_Step1	Distance Max COP-BCOM Step1	Distance_COP-BCOM_at Toe-off	Distance_Total BCOM Displacement_Vertical	Force PeakGRF Posterior (Braking)	Force_Stance-Limb PeakGRF_Vertical	Force_PeakGRF_Vertical	Momentum_Peak BCOM_Vertical		Velocity_Peak BCOM_Vertical		Position_COP_AP_at Seat-off	Position_BCOM_AP_at Seat-off	Time%_ Movement -Onset to Peak BCOM Velocity_Vertical	Time_Movement -Onset to PeakGRF_Posterior	Time_Movement -Onset to PeakGRF_Anterior	Time_Movement -Onset to Peak BCOM Momentum_Vertical	Time_Movement -Onset to Peak BCOM Momentum_Horizontal		Time Movement-Onset to Seat-off (Flexion Mom Time)	Consistent Parameter
Jones et al 2016	Jones et al 2016	Jones et al 2016	Jones et al 2016	Buckley et al 2008	Buckley et al 2008	Jones et al 2016	Jones et al 2016	Buckley <i>et al</i> 2008 Jones <i>et al</i> 2016	Kouta et al 2006	Kerr and Kerr 2001	Magnan et al 1996	Jones et al 2016	Magnan et al 1996	Kouta et al 2006	Jones et al 2016	Buckley et al 2008	Magnan et al 1996	Magnan et al 1996	Kouta et al 2006	Kerr and Kerr 2001	Kerr and Kerr 2001	Magnan et al 1996	Magnan et al 1996	Magnan et al 1996	Buckley <i>et al</i> 2008 Jones <i>et al</i> 2016	Study
STW	STW	STW	STW	STW	STW	STW	STW	STW STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW	STW STW	1
STS*	STS*	STS*	STS*	GI	GI	STS*	STS*	GI*	STS	STS	STS	STS*	STS	STS	STS*	STS	STS	STS	STS	STS	STS	STS	STS	STS	STS STS*	2
0.607 –	0.000 -	0.607 –	0.000 -	-0.782 -	-0.622 –	0.607 -	-0.304 -	-0.514 0.299 -0.137	0.527 –	-0.623 –	0.484 –	-0.607 -	-0.768 –	-0.228	-0.429 -0.415	-0.551	0.070 -	-0.060 -	0.252 -	0.038 -	-0.688 –	0.521 -	0.038 -	0.121	-0.079 0.152 0.055	g M
(-0.257 to 1.472)	(-0.841 to 0.841)	(-0.257 to 1.472)	(-0.841  to  0.841)	(-1.589 to 0.026)	(-1.417 to 0.173)	(-0.257 to 1.472)	(-1.151 to 0.544)	(-0.712 to 0.439)	(-0.375 to 1.428)	(-1.582 to 0.335)	(-0.415 to 1.382)	(-1.472 to 0.257)	(-1.690 to 0.154)		(-0.898 to 0.069)		(-0.813 to 0.953)	(-0.943 to 0.823)	(-0.635 to 1.139)	(-0.892 to 0.968)	(-1.653 to 0.276)	(-0.380 to 1.422)	(-0.844 to 0.921)		(-0.423 to 0.533)	95%CI
0.169	1.000	0.169	1.000	0.058	0.125	0.169	0.483	0.642	0.252	0.202	0.291	0.169	0.102		0.093		0.877	0.894	0.578	0.936	0.162	0.257	0.932		0.823	р

Momentum\_ - refers to a momentum measurement parameter; Position\_ - refers to a position in a certain direction measurement parameter; STS - sit-to-stand; STW - sit-to-walk; Time\_ - refers to a time-related measurement parameter; Velocity\_ - refers to a velocity measurement parameter; \*refers to data from STSW analogous to STS